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# **Robust surface-subsurface modification of PDMS through atmospheric pressure atomic layer deposition**

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# Robust surface-subsurface modification of PDMS through atmospheric pressure atomic layer deposition

Polydimethylsiloxane (PDMS) has been widely employed as a material for microreactors and lab-on-a-chip technologies. However, in its applications, PDMS suffers from two major problems: its weak resistance against common organic solvents and its chemically non-functional surface. To overcome both issues, atmospheric pressure atomic layer deposition (AP-ALD) can be used to deposit an inorganic nano-layer ( $\text{TiO}_x$ ) on PDMS that in turn can be further functionalized. The inorganic nano-layer is previously communicated to durably increase the organic solvent resistance of PDMS. In this study, we investigate the possibility of this  $\text{TiO}_x$  nano-layer in providing surface anchoring groups on PDMS surfaces, enabling further functionalization. We treat PDMS samples cured at three different temperatures with AP-ALD and measure the hydrophilicity of the treated samples as an indicator of the presence of surface anchoring groups. We find that all the treated PDMS samples become hydrophilic right after the AP-ALD treatment. We further find that the AP-ALD-treated PDMS samples cured at  $150^\circ\text{C}$  and  $200^\circ\text{C}$  maintain their hydrophilicity, while the samples cured at  $70^\circ\text{C}$  become less hydrophilic over time. The presence of surface anchoring groups through  $\text{TiO}_x$  nano-layer deposition on PDMS is further demonstrated and utilized by depositing gold nanoparticles (AuNPs) on the AP-ALD-treated samples. The samples exhibit visible light absorbance at 530 nm, a typical absorbance peak for AuNPs. In conclusion, this study demonstrates the use of nano-layers grown by AP-ALD to solve the two major problems of PDMS simultaneously, widening the PDMS applicability, especially for use in high-end applications such as catalysis and bio-sensing.

## 1 Introduction

In the fields of medicine, biology, and chemistry, there is a rising trend of using polydimethylsiloxane (PDMS) as a material for microfluidics and protective coatings [1, 2]. The high transparency, excellent biocompatibility, ease of rapid prototyping, and tunable bulk properties of PDMS make it an attractive substrate, enabling wide selections of optical-based micro-(bio)processing [1, 3, 4]. However, PDMS has two major issues: its weak resistance against organic solvents and its chemically non-functional surface. When it comes in contact with common organic solvents such as chloroform and acetone, PDMS swells and deforms. Furthermore, the PDMS surface is naturally hydrophobic and mostly dominated by methyl groups, making it difficult to introduce functional groups such as hydroxyl, thiol, amine, carboxylic, epoxy rings, and many others [5, 6]. As a result, the use of PDMS is limited, especially in applications where the presence of functional groups or the use of organic solvents is vital [3, 4, 7, 8].

To overcome the limitations of PDMS, researchers explored two main directions: bulk modification and surface treatment [5, 9]. Since bulk modification leads to undesirable changes in PDMS bulk properties (e.g. softer/stiffer, lower transparency), wet and dry surface treatments have been explored [1, 4, 5, 10, 11]. A common dry surface treatment is the use of oxygen plasma to introduce hydroxyl groups on PDMS. While it renders the surface hydrophilic, the surface recovers to its initial hydrophobic state within hours known as hydrophobic recovery [12, 13]. Furthermore, this treatment does not render the surface inert such that oxygen-treated PDMS samples cannot be used for systems involving organic solvents. As such, numerous modifications involving liquid chemistry and sol-gel methods have been developed [14–19]. While using HEMA, PEG, PVP, or PVA solutions to coat the PDMS surface does make the surface more hydrophilic [14–17], the introduced functional group could be desorbed and washed away by many solvents [15]. Furthermore, the PDMS is still susceptible to organic solvents. As an alternative, researchers looked into depositing non-organic layers. Roman and Culbertson used transition metal sol-gel precursors to introduce metal oxide groups [16] while the

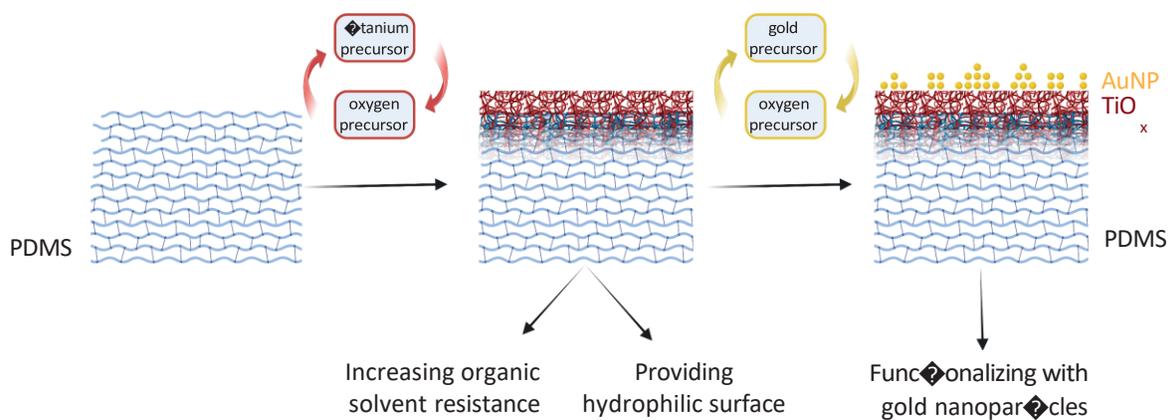


Fig. 1 Illustration of modification of PDMS through deposition of a  $\text{TiO}_x$  nanolayer and further functionalization through the deposition of gold nanoparticles (AuNPs). The deposition of  $\text{TiO}_x$  nano-layers both increases the organic solvent resistance of PDMS and renders the surface hydrophilic through hydroxyl groups. These groups act as anchoring points for further functionalization, here shown for AuNPs.

40 group of Weitz used TEOS and MTES to deposit a glass-like substance on the PDMS surface [19]. While both offer a more robust  
 41 layer to both protect the PDMS from direct organic solvent exposure and provide hydrophilic surface groups, the sol-gel method  
 42 cannot be used to coat complex structures uniformly because the removal of the thick sol-gel solution using gas leaves unwanted  
 43 residues. Apart from being uneven, the microscopically thick coating may compromise the bulk properties [20]. Therefore, vapor  
 44 deposition of inorganic nanoscopically thin layers on PDMS becomes promising due to the use of a single phase in its whole depo-  
 45 sition process while solving both issues of PDMS simultaneously [6, 21–26].

46  
 47 Among all vapor deposition methods, atomic layer deposition is renowned as it faithfully coats complex nanostructures with  
 48 a wide variety of coating materials [27]. Using alternating reactions, the thickness of the coating layer, and its corresponding  
 49 properties [27], can be controlled in a straightforward manner. When it comes to porous substrates including the elastomer PDMS,  
 50 substrate infiltration could occur [26, 28, 29]. Therefore, numerous terms have been coined in order to represent the process better,  
 51 such as multiple pulsed infiltrations, vapor phase infiltration, sequential infiltration synthesis, atomic layer deposition, or atomic  
 52 layer infiltration [30]. In the case of PDMS, we previously communicated that both surface growth and subsurface infiltration  
 53 occur during the atmospheric pressure deposition process [31]. There, we showed that this unique surface-subsurface deposition  
 54 contributes positively to increasing PDMS organic solvent resistance through a coating of titanium oxide [31]. Due to more than  
 55 one phenomenon taking place in our study, in this paper, we also opt to use the more general term atomic layer deposition (ALD).

56  
 57 In this paper, we follow up on our previous work by extending the use of the atmospheric pressure ALD (AP-ALD) of titanium  
 58 oxide ( $\text{TiO}_x$ ) to functionalize the PDMS substrate. While  $\text{TiO}_x$  has been demonstrated to provide a protective layer against organic  
 59 solvent [31], it also has potential in providing hydroxyl groups that act as anchoring points for other molecules or particles [17, 32, 33].  
 60 In this study, we measure the hydrophilicity of the treated samples as an indicator for the functionality. We further demonstrate the  
 61 presence of the surface anchoring groups by functionalizing the treated PDMS surface by depositing gold nanoparticles (AuNPs)  
 62 on top, as illustrated in Figure 1. The presented results show a promising use of AP-ALD to tackle both weaknesses of PDMS in  
 63 one go by increasing the organic solvent resistance and functionalizing the surface robustly while eliminating the need for expensive  
 64 vacuum technology in its fabrication.

## 66 2 Method

### 67 2.1 Substrate preparation

68 PDMS samples were fabricated by mixing the elastomer and curing agent (Sylgard 184 Elastomer Kit, Dow Corning) in a ratio of  
69 10:1. After manual stirring of the mixture for 2 min, trapped air bubbles were removed using a vacuum desiccator for 30 min. The  
70 degassed mixture was poured into a Petri dish and placed in the vacuum desiccator again for another 30 min. PDMS was then  
71 cured in an oven at 70 °C, 150 °C, or 200 °C for at least 10 hours. Samples of 25 mm × 30 mm (0.5 mm thick) were cut from the  
72 cured PDMS and bonded on a glass slide after plasma treatment (oxygen in air, Harrick, PDC-002) at 0.2 - 0.4 mbar for 140 s.

### 73 2.2 Atomic layer deposition of TiO<sub>x</sub> layers

74 TiO<sub>x</sub> was deposited using a home-built atmospheric-pressure setup with a tubular flat-substrate reactor, where the precursor was  
75 delivered parallel to the substrate, as described previously [31]. Tetrakis-dimethylamino titanium (IV) (TDMAT, >99.99% Merck  
76 Sigma) and ozone-enriched air (Sander Certizon) were used as titanium and oxygen precursor respectively, where nitrogen (N<sub>2</sub>  
77 99.999%, Linde) was used as carrier gas. The carrier gas flowed through a bubbler for the metal precursor (kept at 70 °C) at  
78 0.5 L/min for 10 s, while the ozone-enriched air flowed at 0.7 L/min for 30 s. In between, the nitrogen purging was done at 2 L/min  
79 for 100 s. Unless otherwise stated, we performed 100 cycles and kept the chamber at 100 °C. As a comparison to AP-ALD treatment,  
80 we also conducted TiO<sub>x</sub> deposition through thermal atomic layer deposition (Th-ALD) and plasma enhanced atomic layer deposition  
81 (PE-ALD) in a commercial atomic layer deposition reactor (Veeco Fiji G2) at 10<sup>-5</sup> mbar and 100 °C. While TDMAT was used as the  
82 Ti precursor, water and oxygen plasma were used for the oxygen precursor in Th-ALD and PE-ALD, respectively. Both precursors  
83 were introduced into the chamber at 0.02 L/min for 60 ms alternatingly with 45 s (Th-ALD) or 5 s (PE-ALD) of nitrogen purging  
84 done in between. To ensure a fair comparison, we performed 100 cycles at 100 °C.

### 85 2.3 Atomic layer deposition of gold nanoparticles on TiO<sub>x</sub> layers

86 To demonstrate the ability to functionalize the TiO<sub>x</sub>-treated-PDMS-surface, we performed a second AP-ALD in which we deposited  
87 gold nanoparticles (AuNPs) on TiO<sub>x</sub>-treated PDMS samples cured at 150 °C. AuNPs were deposited using trimethylphosphino-  
88 trimethyl gold(III) (6-Me, prepared according to literature procedure [34, 35]) and ozone-enriched air as a precursor for 5 cycles at  
89 100 °C using the same ALD set-up. The nitrogen carrier gas flowed through a bubbler for the metal precursor (kept at 75 °C) at  
90 0.5 L/min for 15 s, while the ozone-enriched air flowed at 0.7 L/min for 30 s. In between, the purging was done at 2 L/min for  
91 100 s. As a control, we also deposited AuNPs on bare PDMS samples with similar operating parameters.

### 92 2.4 Surface characterization of AP-ALD-treated PDMS samples

93 In order to characterize the surface morphology, field emission scanning electron microscopy (FESEM, Hitachi Regulus SU8230)  
94 at a beam current of 1-5 μA and electron energy of 1-10 keV was conducted. To obtain the surface elemental information, X-ray  
95 photoelectron spectroscopy (XPS) (ThermoFisher Scientific Nexsa) equipped with a monochromatic Al K $\alpha$  radiation source and  
96 a pass energy of 30 and 100 eV for the survey scan, and ion-beam etching unit was used. Depth profiling was conducted by  
97 etching the surface using Ar<sup>+</sup> ions (2 keV with a raster size of 2 mm) while a flood gun was used to compensate for the differential  
98 charging. Thermo Advantage 5.913 and CASA-XPS software were used to post-process the XPS peak profile, where the spectra were  
99 charge-corrected with the adventitious carbon peak at 284.8 eV. The thickness of the TiO<sub>x</sub> layer was approximated using an etch  
100 rate obtained in the previous study [31]. This thickness was used to calibrate the etch rate of the TiO<sub>x</sub> layer on PDMS during XPS  
101 measurement, indicating an approximated elemental depth profile.

## 102 2.5 Particle size distribution of the deposited AuNPs

103 To obtain the particle size distribution of AuNPs, ALD-coated PDMS samples were sonicated in HNO<sub>3</sub> 1 M (Merck Sigma) for  
104 15 minutes and left immersed for 48 h to dissolve the TiO<sub>x</sub> layer under the AuNPs and disperse them into the solution. The  
105 solution was then centrifuged (MicroCL 21/21R, Thermoscientific) at 14800 rpm for 10 min and the supernatant was decanted as  
106 much as possible prior to being washed with ethanol (96%) three times and transferred onto Quantifoil copper TEM grids (coated  
107 with carbon). Transmission electron microscopy (TEM) images of the AuNPs were acquired using a JEOL JEM1400 microscope  
108 operating at a voltage of 120 kV working in bright-field mode. The average particle size and particle size distribution (PSD) curves  
109 were obtained using the size of more than 350 individual particles analyzed using ImageJ.

## 110 2.6 Wettability study of TiO<sub>x</sub> coated PDMS samples

111 To quantify the surface wetting property, the dynamic contact angles were measured using a Krüss drop shape analyzer (Figure S1)  
112 at ambient conditions. An automated dispensing system was used to form the droplet and to increase and decrease the volume of  
113 the droplet. After forming a droplet of milliQ-water at a needle and bringing it in close contact with the surface of a PDMS sample,  
114 the droplet formed a contact line with the surface. As the droplet volume increased gradually, the droplet grew bigger while the  
115 contact line remained pinned, resulting in an increase in the contact angle. The maximum contact angle before the droplet was  
116 unpinned and started advancing is referred to as the advancing contact angle ( $\theta_{adv}$ , Figure S1a), After that, the volume of the  
117 droplet was decreased, resulting in again pinning of the contact line and a decrease in contact angle. The minimum contact angle  
118 before the droplet was unpinned and started receding is referred to as the receding contact angle ( $\theta_{rec}$ , Figure S1b). Contact angle  
119 measurements were done a few minutes, 24 h, 48 h, 200 h, 400 h, and 800 h after the samples were taken out of the ALD reactors,  
120 with samples being stored in a glove box to reduce random air contamination during storage. Drop shape analysis software was used  
121 to measure contact angles from camera images. Average values were reported from 10 measurements via the typical uncertainty (2  
122 s.d.).

## 123 2.7 Washing of the PDMS samples and ATR-FTIR characterization

124 To examine our hypothesis about the presence of uncured monomer in PDMS that diffuses out and compromises the AP-ALD  
125 coating, we pre-washed the PDMS samples to remove the non-crosslinked molecules from the PDMS[36]. The PDMS samples were  
126 soaked in 70 mL cyclohexane (99% vol, Merck Sigma), for 72 h. Hereafter, the washing solvent was taken out and kept for infrared  
127 spectroscopy measurement, and a second soaking step of the PDMS samples was conducted for 24 h. After measuring the weight of  
128 the swollen PDMS samples, the samples were dried at room temperature for at least 8 h. The dried PDMS samples were weighed  
129 again to calculate the weight loss during the washing. The ATR-FTIR (attenuated total reflectance Fourier-transform infra-Red  
130 spectroscopy) measurements on the washing solvents were performed on a NEXUS from Thermo Nicolet instrument equipped with  
131 a liquid Nitrogen cooled MCT detector with a wavelength range of 4000 to 500 cm<sup>-1</sup>.

## 132 2.8 UV-Vis spectrophotometry study

133 To measure the photonic effect of the TiO<sub>x</sub>-treated PDMS surface functionalized with AuNPs, light absorption was measured with  
134 a wide scan reading (300 - 800 nm) using a NanoDrop™ 2000/2000c spectrophotometer. The reported value was an average of 3  
135 measurements via the typical uncertainty (2 s.d.).

### 137 3 Result and Discussion

#### 138 3.1 Simultaneous surface and subsurface growth in AP-ALD

139 Before examining the treated samples, we point out that deposition of  $\text{TiO}_x$  on PDMS may result in both surface and subsurface  
 140 growth, and therefore is more ambiguous to characterize [31]. Figure 2a shows the relative atomic percentage of titanium changes  
 141 along the depth of the PDMS samples obtained using the XPS depth profiling method, while Figure 2b shows the corresponding XPS  
 142 surface composition. On all samples, a significant percentage of Ti is observed on the surface, even to an etch depth of  $\sim 70$ -80 nm,  
 143 indicating the formation of the  $\text{TiO}_x$  layer. A closer look at Figure 2b confirms that the atomic ratio of titanium to oxygen is  
 144 about 1 to 2, indicating  $\text{TiO}_2$  deposition. The titanium atomic percentage of all samples gradually declines in a comparable manner  
 145 along the etch depth, before dropping to a percentage of  $\sim 5\%$  at the depth of 200 nm. This gradual decline indicates the formation  
 146 of an infiltrated layer. This result is in good agreement with previous results [31]. For all three AP-ALD samples, we observe  
 147 similar profiles, indicating that the curing temperature has no effect on the resulting surface-subsurface structure. This is expected  
 148 because the average size of the pores in PDMS is in the range of a few tens nm to a few  $\mu\text{m}$  [37], much larger than the size of the  
 149 precursor molecules. Thus, irrespective of the relative difference between the pore sizes due to differences in cross-linking densities,  
 150 the penetration behavior of the precursor is the same in all three samples. Additionally, we study the effect of the number of cycles  
 151 on the depth profile. We find that the  $\text{Ti}2p$  signal is not detected on the samples deposited with 10 cycles, while an appreciable  
 152 signal is detected after 20 cycles (Figure S2a), indicating the presence of nucleation delay, which is typical for non-reactive substrates  
 153 such as PDMS [24, 26, 31]. Furthermore, the surface and subsurface growth seem to occur simultaneously (Figure S2b), as a higher  
 154 number of ALD cycles leads to both a thicker  $\text{TiO}_x$  layer and a more moderate, deeper infiltration. Besides the XPS analysis of  
 155 the surface and subsurface, an analysis of the surface FE-SEM shows that the coating is visually smooth without nano-cracks, even  
 156 after 800 h, indicating a stable  $\text{TiO}_x$  layer (Figure S3).

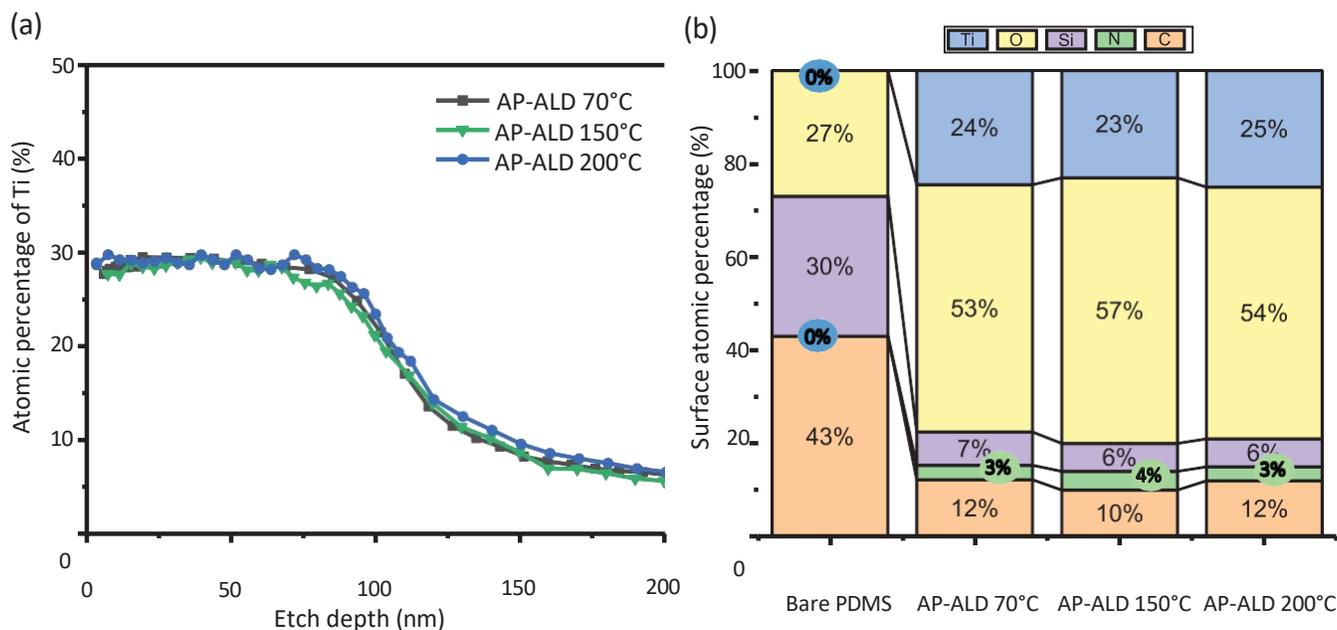


Fig. 2 (a) XPS depth profiling showing the relative atomic percentage of titanium in the surface and subsurface of AP-ALD-coated PDMS samples cured at 70°C, 150°C, 200°C, and (b) XPS elemental analysis of the surface.

### 157 3.2 Hydrophilicity as indicator of functional surface

158 We use hydrophilicity as an indicator for the presence of surface-anchoring groups (in this case hydroxyl groups) on the ALD-coated  
 159 PDMS surfaces. More specifically, we use the contact angle of a droplet of water brought into contact with the coated surfaces.  
 160 Although the observed angle depends on the way of contacting, it is bounded by the contact angle hysteresis range, with an upper  
 161 and lower bound intrinsic to the surface. The upper bound, called the advanced contact angle, is taken as the relevant characteristic  
 162 in this work. The advancing contact angle ( $\theta_{adv}$ ) measurement of bare PDMS and AP-ALD-coated PDMS samples cured at different  
 163 temperatures are presented in Figure 3a. Directly after coating ( $t=0$ ), the (three) bare PDMS samples show a similar advancing  
 164 contact angle at  $118^\circ \pm 1^\circ$ , in accordance with reported values [38, 39]. The AP-ALD-coated PDMS samples exhibit a significantly  
 165 lower  $\theta_{adv}$ , around  $68^\circ \pm 4^\circ$  at  $t=0$ . A closer look at the XPS surface composition of these samples shows a high  $\text{TiO}_x$  coverage  
 166 (Figure 2b), indicating that the hydrophilicity of the samples depends on the composition and possibly on the structure of the  $\text{TiO}_x$   
 167 coating. To confirm, we conducted two additional types of ALD treatment on PDMS samples, plasma enhanced ALD (PE-ALD)  
 168 and thermal ALD (Th-ALD), that are known to yield notably different  $\text{TiO}_x$  layers [31]: PE-ALD leads to a  $\text{TiO}_x$  layer on top  
 169 of the PDMS surface, while Th-ALD leads to a  $\text{TiO}_x$  layer inside the PDMS (infilling). As expected, the PE-ALD-coated PDMS  
 170 samples exhibit a  $\theta_{adv}$  at  $69^\circ \pm 1^\circ$  that is comparable to the AP-ALD-coated PDMS samples (Figure S4a). This result is in line with  
 171 the previous finding by Pessoa [23]. By contrast, the Th-ALD-coated PDMS samples exhibit a  $\theta_{adv}$  at  $111^\circ \pm 2^\circ$  that is comparable  
 172 to bare PDMS samples (Figure S4a). When looking at the surface elemental composition (Figure S4b), the XPS surface spectra of  
 173 PE-ALD-, Th-ALD-, and AP-ALD-coated PDMS samples show the expected profile of the  $\text{TiO}_x$  layers [31]. Both PE-ALD- and  
 174 AP-ALD-coated samples show a dominance of  $\text{Ti}2p$  peak with little  $\text{C}1s$  and  $\text{Si}2p$  peaks, indicating high coverage of  $\text{TiO}_x$  layers.  
 175 On the other hand, the Th-ALD-coated samples show a dominance of  $\text{C}1s$  and  $\text{Si}2p$  peaks with little  $\text{Ti}2p$  peak instead, typical  
 176 elements found in PDMS molecular chains. These observations underline the importance of the type of  $\text{TiO}_x$  layer, and the type of  
 177 ALD treatment used, on the hydrophilicity of the coated PDMS samples.

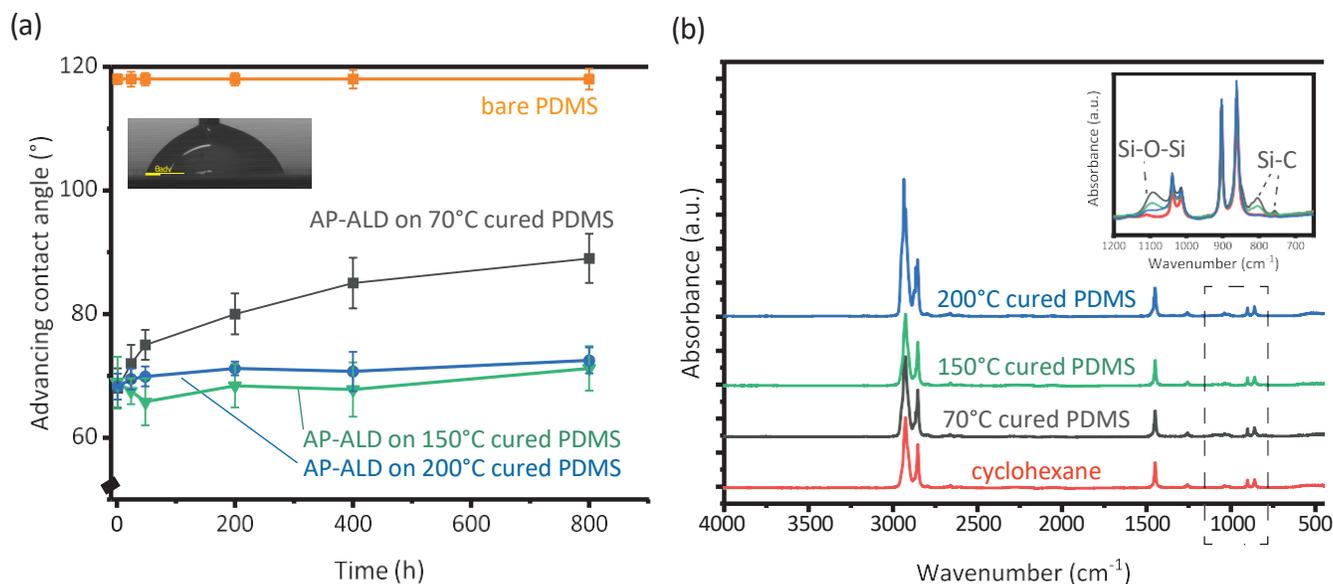


Fig. 3 (a) Advancing contact angle measurement on bare and AP-ALD-coated PDMS cured at three different temperatures and (b) ATR-FTIR spectra of the solvent (cyclohexane) used to wash PDMS samples cured at different temperatures together with a control (pure cyclohexane).

178 A well-known phenomenon in the coating of PDMS samples is the gradual temporal change in surface composition leading to the  
 179 recovery of the hydrophobicity [22]. To test the robustness of the AP-ALD treatment, we measured the advancing contact angle on  
 180 the same samples over prolonged periods of time. While the hydrophobicity of the bare PDMS samples is constant in time, we find

181 that  $\theta_{adv}$  of AP-ALD-coated PDMS samples cured at 70 °C increases along the duration of the measurement, reaching 89 ° ± 4 ° after  
182 800 h (Figure 3a). This increase is significantly lower when compared to PE-ALD coated PDMS samples cured at 70 °C (reaching  
183 103 ° ± 1 ° after 800 h, see Figure S4a). We argue that the combined surface-subsurface TiO<sub>x</sub> layer obtained through AP-ALD acts  
184 as a barrier for the out-diffusion of uncured monomers, slowing down the hydrophobic recovery as compared to the surface-only  
185 TiO<sub>x</sub> layer obtained through PE-ALD. This is in line with the observation that the surface-subsurface TiO<sub>x</sub> layer obtained through  
186 AP-ALD shows no visual cracks (Figure S3), while nano cracks have been reported in the surface-only TiO<sub>x</sub> layer obtained through  
187 PE-ALD [31]. While these nano cracks do not affect the hydrophilicity of the PE-ALD-coated samples at t=0 (Figure S4a), it  
188 becomes a route for the uncured monomers to out diffuse, leading to hydrophobic recovery after 800 h.

189

190 The AP-ALD coating on PDMS samples cured at 70 °C renders the surface hydrophilic over prolonged times, yet it is subject to  
191 change due to the out-diffusion of uncured monomers. Earlier studies have suggested that curing of PDMS at higher temperature  
192 changes the internal crosslinking of PDMS, leading to a tighter network [40] and fewer low-molecular-weight molecules [41]. For  
193 the AP-ALD-coated PDMS samples cured at 150 °C and 200 °C, we indeed observe a negligible increase of advancing contact angle,  
194 from 69 ° ± 4 ° after coating to 71 ° ± 4 ° after 800 h for 150 °C, and from 68 ° ± 2 ° after coating to 73 ° ± 2 ° after 800 h for 200 °C (Figure  
195 3a). Another way to reduce the amount of uncured monomer present in PDMS samples is to wash the cured PDMS samples using  
196 a solvent. The ATR-FTIR spectra of the solvent used to wash PDMS samples cured at 70 °C, 150 °C, and 200 °C show elevated  
197 peaks associated with the Si-O-Si and Si-C bonds in reference to the spectrum of the pure solvent [6, 22, 42], with the amount  
198 of uncured monomer decreasing with increasing curing temperature (Figure 3b). As expected, the advancing contact angle of the  
199 AP-ALD-coated PDMS samples cured at 70 °C and washed prior to ALD show a reduction in hydrophobic recovery, reaching 80 ° ± 4 °  
200 after 800 h. Given that the surface of the AP-ALD-coated PDMS samples cured at 150 °C and 200 °C remains stable, washing with  
201 solvent is expected to have a little gain. Indeed, the advancing contact angle after 800 h is 70 ° ± 3 ° and 70 ° ± 3 °, respectively, similar  
202 to the non-washed samples. To confirm that this gain is exclusive to only AP-ALD-coated samples, we carried out an additional  
203 experiment by coating the PDMS samples cured at 150 °C with PE-ALD. The advancing contact angle after 800 h is 94 ° ± 4 °, with  
204 the hydrophobic recovery attributed to cracks in the TiO<sub>x</sub> coating [31]. This shows that both curing at temperature 150 °C and  
205 200 °C and deposition of an (intact) surface-subsurface layer through AP-ALD are essential in obtaining a stable hydrophilic TiO<sub>x</sub>  
206 coating on PDMS.

207

### 208 3.3 Demonstration of functional surface

209 To demonstrate the ability to functionalize the PDMS surface, we deposit gold nanoparticles (AuNPs) on AP-ALD-coated PDMS  
210 samples. Figure 4a shows the presence of AuNPs on the PDMS samples sequentially coated with the Ti and Au precursors (indicated  
211 by Au4f signal in Figure 4a, inset), while no appreciable Au4f signal is found on the control PDMS sample coated with only Au  
212 precursor that shows no AuNPs (Figure 4b). The post-processing of the signal (Figure S5a, calibrated with C1s peak at 248.8eV)  
213 shows the presence of mostly Au (o) at the peak of 84.4eV and 88.1eV, a well-separated spin-orbit component of 3.7eV. From the  
214 comparison, the presence of the (stable) TiO<sub>x</sub> layer on the PDMS is critical in providing reactive groups for initiating gold-based  
215 ALD. Furthermore, to check the purity of the formed AuNP, an extra scan is conducted on P2p binding energy range as phosphorus  
216 is an identifiable element in the ALD Au precursor ligand. Figure S5b shows that the P2p signal is below the detection limit, sug-  
217 gesting the absence of AP-ALD by-products or the remaining ligands. We examine the photonic performance of the AuNP-coated  
218 sample by measuring the diffuse surface reflectance of the sample within UV-Vis. A clear peak of 530 nm is observed (Figure 4c),  
219 corresponding to a typical local surface plasmon resonance of AuNPs [43]. We confirm that this peak is not seen in bare PDMS  
220 samples and TTiO<sub>x</sub>-coated PDMS samples. To characterize the particle size distribution, the AuNPs are dispersed by dissolving  
221 the underlying TiO<sub>x</sub> layer first using HNO<sub>3</sub> 1 M, before being washed with ethanol and placed on a TEM grit. The processed image

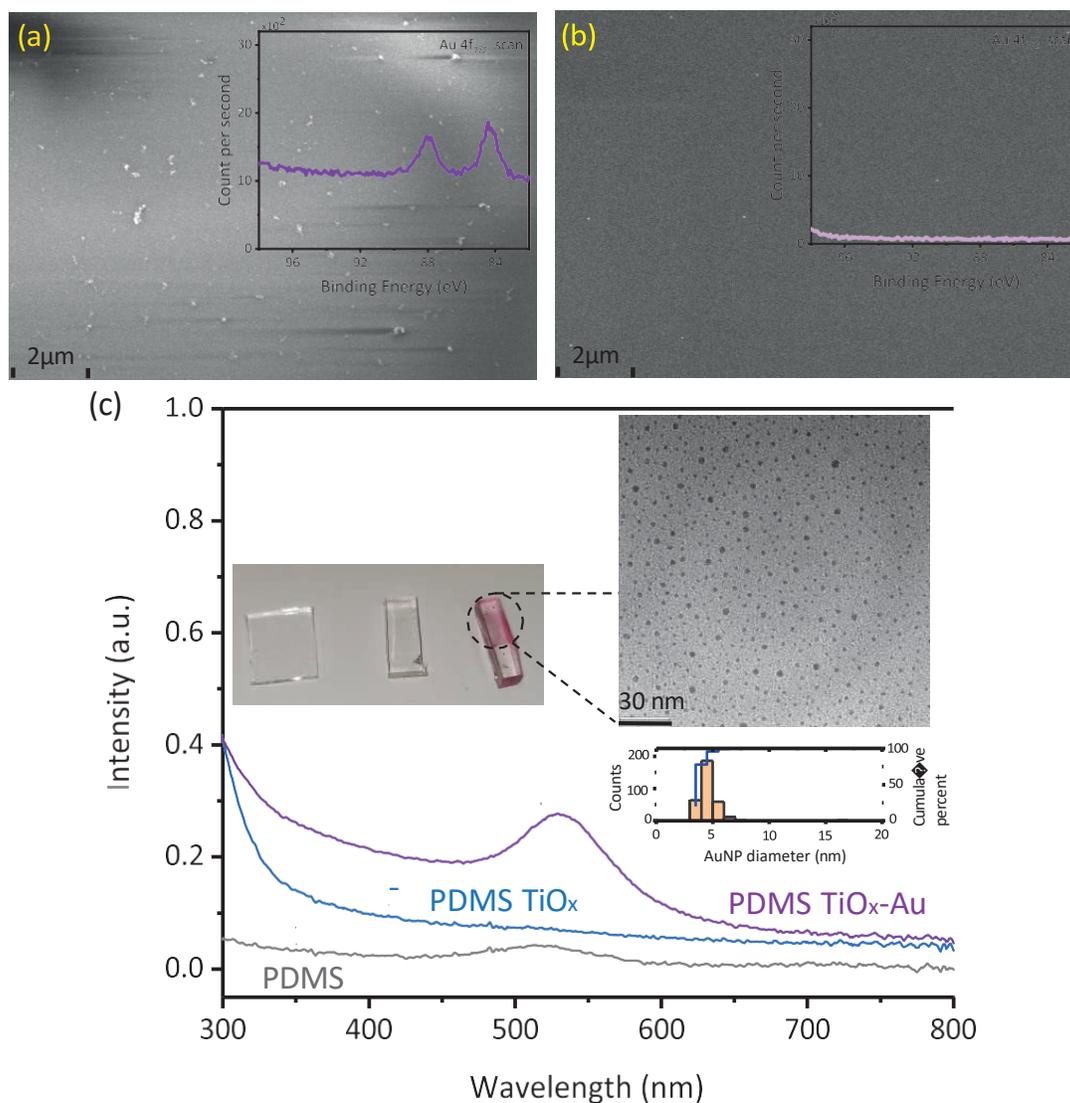


Fig. 4 Scanning electron microscopy image of PDMS samples coated with 5 cycles of Au precursors preceded by (a) 100 cycles and (b) 0 cycles of Ti precursors on PDMS samples cured at 150 °C. Both AP-ALD processes were conducted at 100 °C. The insets show the corresponding XPS spectra at the typical Au4f binding energy range. (c) UV-Vis spectra of PDMS, PDMS coated with TiO<sub>x</sub>, and PDMS coated with TiO<sub>x</sub> and AuNPs. The insets show a photograph of the three samples, a TEM image of the TiO<sub>x</sub>-AuNPs-coated PDMS sample, and the corresponding particle size distribution of the AuNPs.

222 (Figure 4c, inset) shows an average size (diameter) and width of the size distribution of 4.57 nm and a standard deviation of 0.67 nm  
 223 accordingly. This AuNPs size with a relatively narrow size distribution is of interest in many applications including photocatalysis  
 224 and biosensing [44, 45].

225

## 226 4 Conclusion and outlook

227 In conclusion, we show that a nanolayer of metal oxide can be deposited on the transparent soft elastomer PDMS, providing it  
 228 with the necessary hydroxyl groups to allow further functionalization of the surface. We find that the surface-subsurface TiO<sub>x</sub> layer  
 229 obtained through atmospheric pressure ALD is critical in providing a surface that remains hydrophilic and stable over prolonged  
 230 periods of time, with reduced out-diffusion of uncured monomer. For stable hydrophilic TiO<sub>x</sub> layers that do not display hydrophobic

231 recovery, curing of PDMS at a temperature of at least 150 °C is found to be of key importance. We illustrate the further functional-  
232 ization of the TiO<sub>x</sub> -coated PDMS surfaces by depositing gold nanoparticles, also through ALD, opening the opportunity window  
233 to high-end applications.

234

## 235 5 Acknowledgment and conflict of interest

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239

## 240 Notes and references

- 241 1 Kiran Raj M and Suman Chakraborty. Pdms microfluidics: A mini review. *Journal of Applied Polymer Science*, 137(27):48958, 2020.
- 242 2 Ubong Eduok, Omar Faye, and Jerzy Szpunar. Recent developments and applications of protective silicone coatings: A review of pdms functional  
243 materials. *Progress in Organic Coatings*, 111:124–163, 2017.
- 244 3 Inês Miranda, Andrews Souza, Paulo Sousa, João Ribeiro, Elisabete MS Castanheira, Rui Lima, and Graça Minas. Properties and applications of  
245 pdms for biomedical engineering: A review. *Journal of Functional Biomaterials*, 13(1):2, 2021.
- 246 4 Marc P Wolf, Georgette B Salieb-Beugelaar, and Patrick Hunziker. Pdms with designer functionalities—properties, modifications strategies, and  
247 applications. *Progress in Polymer Science*, 83:97–134, 2018.
- 248 5 Amid Shakeri, Shadman Khan, and Tohid F Didar. Conventional and emerging strategies for the fabrication and functionalization of pdms-based  
249 microfluidic devices. *Lab on a Chip*, 21(16):3053–3075, 2021.
- 250 6 Bo Gong, Joseph C Spagnola, and Gregory N Parsons. Hydrophilic mechanical buffer layers and stable hydrophilic finishes on polydimethylsiloxane  
251 using combined sequential vapor infiltration and atomic/molecular layer deposition. *Journal of Vacuum Science & Technology A: Vacuum, Surfaces,*  
252 *and Films*, 30(1):01A156, 2012.
- 253 7 Chao Wang, Mei Liu, Zhifei Wang, Song Li, Yan Deng, and Nongyue He. Point-of-care diagnostics for infectious diseases: From methods to devices.  
254 *Nano Today*, 37:101092, 2021.
- 255 8 Fahima Akther, Shazwani Binte Yakob, Nam-Trung Nguyen, and Hang T Ta. Surface modification techniques for endothelial cell seeding in pdms  
256 microfluidic devices. *Biosensors*, 10(11):182, 2020.
- 257 9 Jian Liu, Yin Yao, Xiaohong Li, and Zhijun Zhang. Fabrication of advanced polydimethylsiloxane-based functional materials: Bulk modifications  
258 and surface functionalizations. *Chemical Engineering Journal*, 408:127262, 2021.
- 259 10 Jinwen Zhou, Dmitriy A Khodakov, Amanda V Ellis, and Nicolas H Voelcker. Surface modification for pdms-based microfluidic devices. *Elec-*  
260 *trophoresis*, 33(1):89–104, 2012.
- 261 11 Zeyad Almutairi, Carolyn L Ren, and Leonardo Simon. Evaluation of polydimethylsiloxane (pdms) surface modification approaches for microfluidic  
262 applications. *Colloids and Surfaces A: Physicochemical and Engineering Aspects*, 415:406–412, 2012.
- 263 12 Dhananjay Bodas and Chantal Khan-Malek. Hydrophilization and hydrophobic recovery of pdms by oxygen plasma and chemical treatment—an  
264 sem investigation. *Sensors and Actuators B: Chemical*, 123(1):368–373, 2007.
- 265 13 Mehrnaz Amerian, Mahshid Amerian, Mahyar Sameti, and Ehsan Seyedjafari. Improvement of pdms surface biocompatibility is limited by the  
266 duration of oxygen plasma treatment. *Journal of Biomedical Materials Research Part A*, 107(12):2806–2813, 2019.
- 267 14 Samu Hemmilä, Juan V Cauich-Rodríguez, Joose Kreutzer, and Pasi Kallio. Rapid, simple, and cost-effective treatments to achieve long-term  
268 hydrophilic pdms surfaces. *Applied Surface Science*, 258(24):9864–9875, 2012.
- 269 15 Tatiana Trantidou, Yuval Elani, Edward Parsons, and Oscar Ces. Hydrophilic surface modification of pdms for droplet microfluidics using a simple,  
270 quick, and robust method via pva deposition. *Microsystems & Nanoengineering*, 3(1):1–9, 2017.
- 271 16 Gregory T Roman, Tyler Hlaus, Kevin J Bass, Todd G Seelhammer, and Christopher T Culbertson. Sol- gel modified poly (dimethylsiloxane)  
272 microfluidic devices with high electroosmotic mobilities and hydrophilic channel wall characteristics. *Analytical Chemistry*, 77(5):1414–1422, 2005.
- 273 17 J-B Orhan, VK Parashar, J Flueckiger, and MAM Gijs. Internal modification of poly (dimethylsiloxane) microchannels with a borosilicate glass  
274 coating. *Langmuir*, 24(16):9154–9161, 2008.
- 275 18 Gregory T Roman and Christopher T Culbertson. Surface engineering of poly (dimethylsiloxane) microfluidic devices using transition metal sol- gel  
276 chemistry. *Langmuir*, 22(9):4445–4451, 2006.
- 277 19 Adam R Abate, Daeyeon Lee, Thao Do, Christian Holtze, and David A Weitz. Glass coating for pdms microfluidic channels by sol–gel methods.  
278 *Lab on a Chip*, 8(4):516–518, 2008.
- 279 20 Hedieh Fallahi, Jun Zhang, Hoang-Phuong Phan, and Nam-Trung Nguyen. Flexible microfluidics: Fundamentals, recent developments, and applica-  
280 tions. *Micromachines*, 10(12):830, 2019.
- 281 21 Hsien-Yeh Chen, Yaseen Elkasabi, and Joerg Lahann. Surface modification of confined microgeometries via vapor-deposited polymer coatings. *Journal*  
282 *of the American Chemical Society*, 128(1):374–380, 2006.
- 283 22 Joseph C Spagnola, Bo Gong, and Gregory N Parsons. Surface texture and wetting stability of polydimethylsiloxane coated with aluminum oxide at  
284 low temperature by atomic layer deposition. *Journal of Vacuum Science & Technology A: Vacuum, Surfaces, and Films*, 28(6):1330–1337, 2010.
- 285 23 RS Pessoa, VP dos Santos, SB Cardoso, ACOC Doria, FR Figueira, BVM Rodrigues, GE Testoni, MA Fraga, FR Marciano, AO Lobo, et al.

- 286 Tio<sub>2</sub> coatings via atomic layer deposition on polyurethane and polydimethylsiloxane substrates: Properties and effects on *C. albicans* growth and  
 287 inactivation process. *Applied Surface Science*, 422:73–84, 2017.
- 288 24 Eun Young Choi, Ju-Hee Kim, Bu-Jong Kim, Ji Hun Jang, Jincheol Kim, and Nochang Park. Development of moisture-proof polydimethylsilox-  
 289 ane/aluminum oxide film and stability improvement of perovskite solar cells using the film. *RSC Advances*, 9(21):11737–11744, 2019.
- 290 25 Sasha Hoshian, Ville Jokinen, and Sami Franssila. Robust hybrid elastomer/metal-oxide superhydrophobic surfaces. *Soft Matter*, 12(31):6526–6535,  
 291 2016.
- 292 26 Sarah Hashemi Astaneh, Gregory Jursich, Cortino Sukotjo, and Christos G Takoudis. Surface and subsurface film growth of titanium dioxide on  
 293 polydimethylsiloxane by atomic layer deposition. *Applied Surface Science*, 493:779–786, 2019.
- 294 27 H Van Bui, F Grillo, and JR Van Ommen. Atomic and molecular layer deposition: off the beaten track. *Chemical Communications*, 53(1):45–71,  
 295 2017.
- 296 28 Inbal Weisbord, Neta Shomrat, Rotem Azoulay, Alexander Kaushansky, and Tamar Segal-Peretz. Understanding and controlling polymer–  
 297 organometallic precursor interactions in sequential infiltration synthesis. *Chemistry of Materials*, 32(11):4499–4508, 2020.
- 298 29 Emily K McGuinness, Fengyi Zhang, Yao Ma, Ryan P Lively, and Mark D Losego. Vapor phase infiltration of metal oxides into nanoporous polymers  
 299 for organic solvent separation membranes. *Chemistry of Materials*, 31(15):5509–5518, 2019.
- 300 30 Thiry Damien Pinson, Jean. *Surface Modification of Polymers - Methods and Applications*, chapter 5 Atomic Layer Deposition and Vapor Phase  
 301 Infiltration, pages 135–157. Number 978-3-527-34541-0. John Wiley & Sons, 2020.
- 302 31 Albert Santoso, Afke Damen, J Ruud van Ommen, and Volkert van Steijn. Atmospheric pressure atomic layer deposition to increase organic solvent  
 303 resistance of pdms. *Chemical Communications*, 58(77):10805–10808, 2022.
- 304 32 Xiaolan Kang, Sihang Liu, Zideng Dai, Yunping He, Xuezhi Song, and Zhenquan Tan. Titanium dioxide: from engineering to applications. *Catalysts*,  
 305 9(2):191, 2019.
- 306 33 Xuanyong Liu, Paul K Chu, and Chuanxian Ding. Surface modification of titanium, titanium alloys, and related materials for biomedical applications.  
 307 *Materials Science and Engineering: R: Reports*, 47(3-4):49–121, 2004.
- 308 34 Matthew BE Griffiths, Peter J Pallister, David J Mandia, and Seán T Barry. Atomic layer deposition of gold metal. *Chemistry of Materials*, 28(1):  
 309 44–46, 2016.
- 310 35 Fatemeh SM Hashemi, Fabio Grillo, Vikram R Ravikumar, Dominik Benz, Ankit Shekhar, Matthew BE Griffiths, Seán T Barry, and J Ruud  
 311 Van Ommen. Thermal atomic layer deposition of gold nanoparticles: controlled growth and size selection for photocatalysis. *Nanoscale*, 12(16):  
 312 9005–9013, 2020.
- 313 36 José González-Rivera, Rossella Iglio, Giuseppe Barillaro, Celia Duce, and Maria Rosaria Tinè. Structural and thermoanalytical characterization of  
 314 3d porous pdms foam materials: the effect of impurities derived from a sugar templating process. *Polymers*, 10(6):616, 2018.
- 315 37 Deyong Zhu, Stephan Handschuh-Wang, and Xuechang Zhou. Recent progress in fabrication and application of polydimethylsiloxane sponges.  
 316 *Journal of Materials Chemistry A*, 5(32):16467–16497, 2017.
- 317 38 Alvaro Mata, Aaron J Fleischman, and Shuvo Roy. Characterization of polydimethylsiloxane (pdms) properties for biomedical micro/nanosystems.  
 318 *Biomedical microdevices*, 7(4):281–293, 2005.
- 319 39 Rian Seghir and Steve Arscott. Extended pdms stiffness range for flexible systems. *Sensors and Actuators A: Physical*, 230:33–39, 2015.
- 320 40 Kyle Berean, Jian Zhen Ou, Majid Nour, Kay Latham, Chris McSweeney, David Paull, Andri Halim, Sandra Kentish, Cara M Doherty, Anita J  
 321 Hill, et al. The effect of crosslinking temperature on the permeability of pdms membranes: Evidence of extraordinary co<sub>2</sub> and ch<sub>4</sub> gas permeation.  
 322 *Separation and Purification Technology*, 122:96–104, 2014.
- 323 41 David T Eddington, John P Puccinelli, and David J Beebe. Thermal aging and reduced hydrophobic recovery of polydimethylsiloxane. *Sensors and  
 324 Actuators B: Chemical*, 114(1):170–172, 2006.
- 325 42 Keil J Regehr, Maribella Domenech, Justin T Koepsel, Kristopher C Carver, Stephanie J Ellison-Zelski, William L Murphy, Linda A Schuler, Elaine T  
 326 Alarid, and David J Beebe. Biological implications of polydimethylsiloxane-based microfluidic cell culture. *Lab on a Chip*, 9(15):2132–2139, 2009.
- 327 43 Seong Youl Lee, Dooho Kang, Sehee Jeong, Hoang Tung Do, and Joon Heon Kim. Photocatalytic degradation of rhodamine b dye by tio<sub>2</sub> and  
 328 gold nanoparticles supported on a floating porous polydimethylsiloxane sponge under ultraviolet and visible light irradiation. *ACS omega*, 5(8):  
 329 4233–4241, 2020.
- 330 44 Sina Witzel, A Stephen K Hashmi, and Jin Xie. Light in gold catalysis. *Chemical Reviews*, 121(14):8868–8925, 2021.
- 331 45 Peng Si, Nasrin Razmi, Omer Nur, Shipra Solanki, Chandra Mouli Pandey, Rajinder K Gupta, Bansi D Malhotra, Magnus Willander, and Adam  
 332 de la Zerda. Gold nanomaterials for optical biosensing and bioimaging. *Nanoscale Advances*, 3(10):2679–2698, 2021.

333 6 Supplementary Information

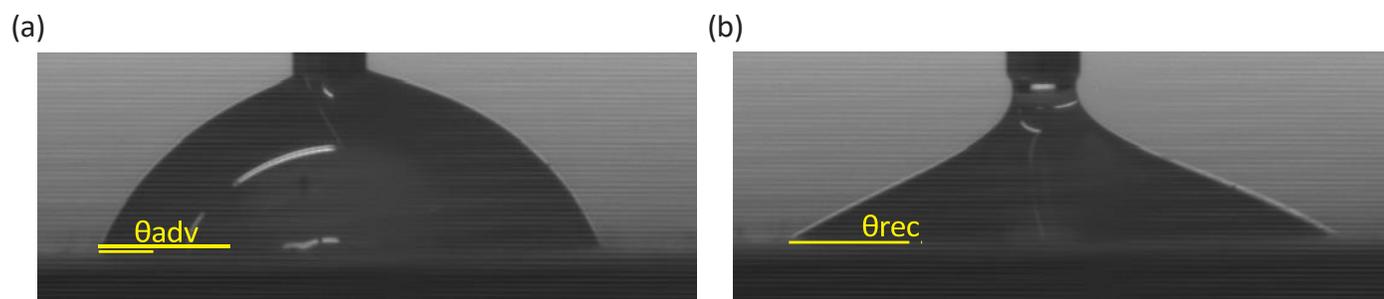


Fig. S1 Measurement of the advancing (right) and receding contact angle (left) on AP-ALD-treated PDMS samples. In the main manuscript, we report the advancing contact angles.

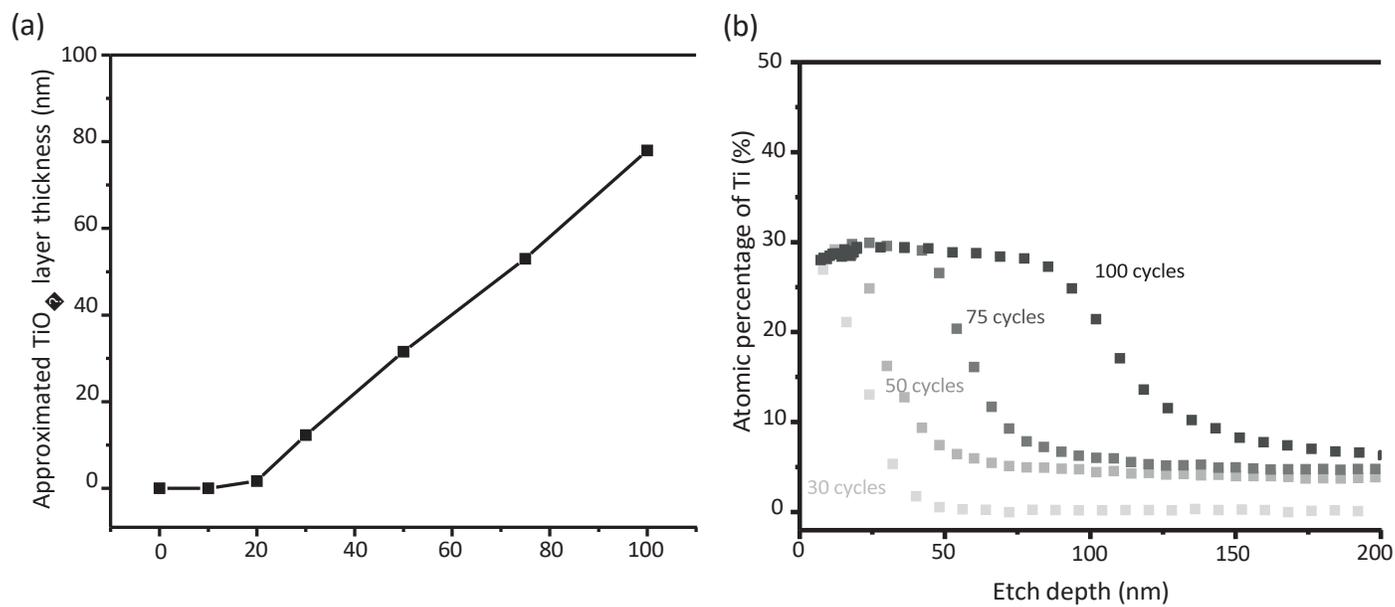
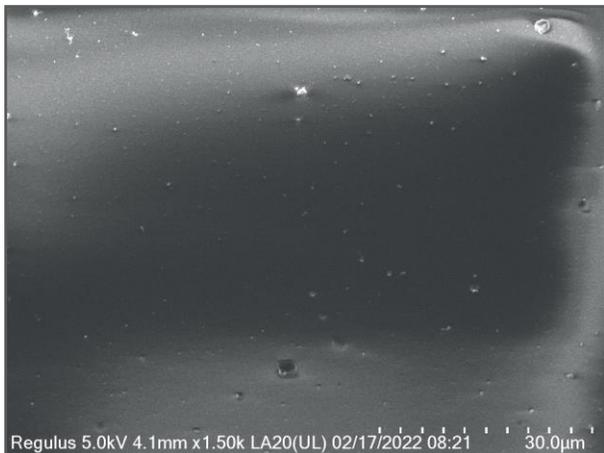
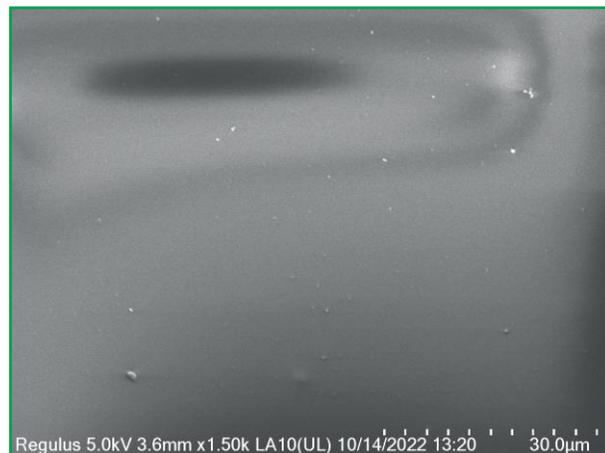


Fig. S2 (a) Approximated  $\text{TiO}_x$  layer thickness obtained from XPS depth profiling with the etch rate determined using a  $\text{TiO}_x$  layer on a silicon wafer as described previously [31]. (b) XPS depth profiling of AP-ALD coated PDMS samples for 30, 50, 75, and 100 cycles. All PDMS samples are cured at  $150^\circ\text{C}$ .

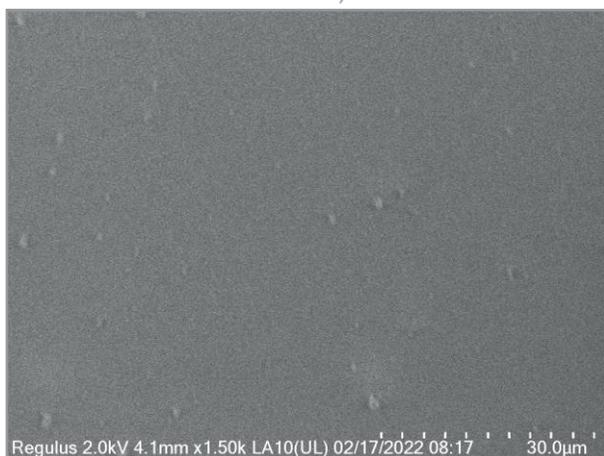
AP-ALD on PDMS cured at 70°C



AP-ALD on PDMS cured at 150°C



AP-ALD on washed PDMS, cured at 70°C



AP-ALD on PDMS cured at 200°C

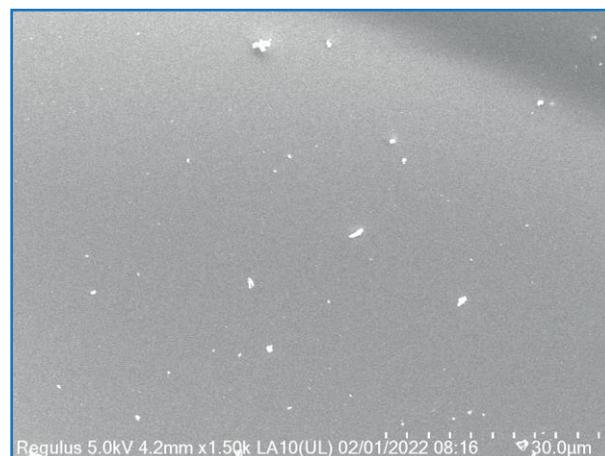


Fig. S3 Scanning electron microscopy images of AP-ALD treated PDMS samples after 800 h. Both of the left images were cured at 70°C (the lower figure was washed in cyclohexane before AP-ALD treatment), and the right images were cured at 150°C, and 200°C (lower).

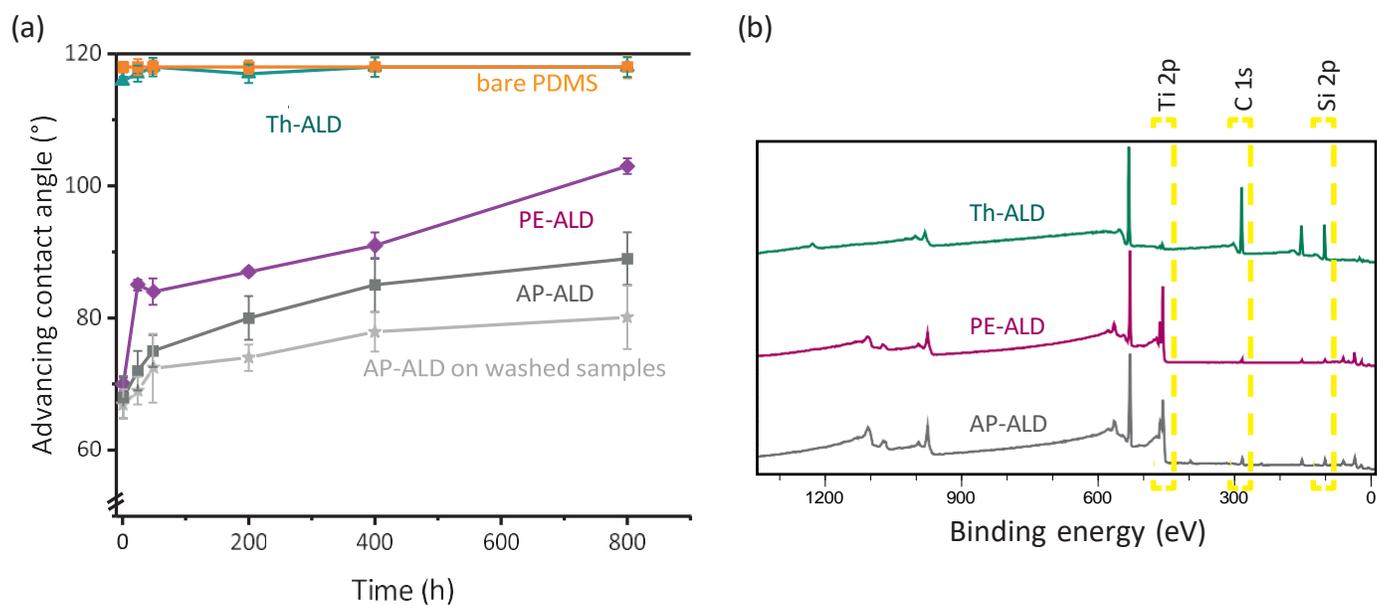


Fig. S4 (a) Advancing contact angle measurement on bare PDMS and PDMS coated with PE-ALD, Th-ALD, and AP-ALD. AP-ALD is also performed on washed samples. All PDMS samples were cured at 70 °C. (b) Corresponding XPS surface spectra of the ALD-coated PDMS samples. The XPS spectra show a high presence of Si2p peak and a low presence of Ti2p peak on Th-ALD samples, indicating minimum TiO<sub>x</sub> surface coverage. The PE-ALD and AP-ALD samples show the opposite, indicating high TiO<sub>x</sub> surface coverage.

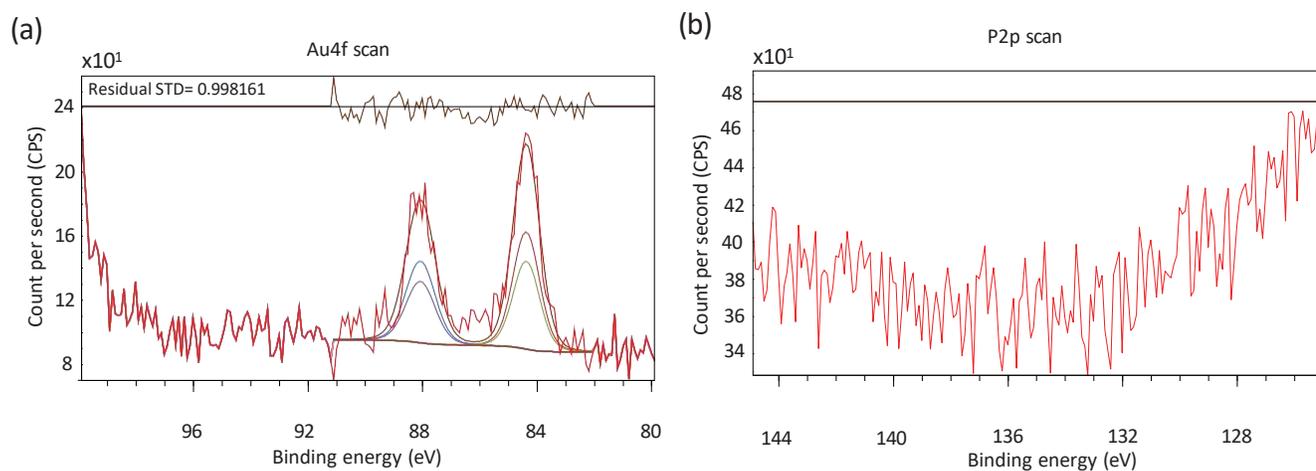


Fig. S5 XPS spectrum of (a) Au4f, (b) P2p of coated PDMS samples. The samples were coated with 100 cycles of Ti precursors and 5 cycles of Au precursors. The horizontal line gives the baseline for the background signal. No clear peak of P2p was observed at the measured binding energy range.